Description of Breast Morphology through Bag of Normals Representation

Dario Allegra¹, Filippo L.M. Milotta¹, Diego Sinitò¹, Filippo Stanco¹, Giovanni Gallo¹, Wafa Taher², and Giuseppe Catanuto³

¹ Department of Mathematics and Computer Science University of Catania, Italy {allegra, milotta, dsinito, fstanco, gallo}@dmi.unict.it ² Fellow of the International Fellowship Querci della Rovere misswtaher@yahoo.com ³ Multidisciplinary Breast Unit Azienda Ospedaliera Cannizzaro, Italy giuseppecatanuto@gmail.com

Abstract. In this work we focus on digital shape analysis of breast models to assist breast surgeon for medical and surgical purposes. A clinical procedure for female breast digital scan is proposed. After a manual ROI definition through cropping, the meshes are automatically processed. The breasts are represented exploiting "bag of normals" representation, resulting in a 64-d descriptor. PCA is computed and the obtained first 2 principal components are used to plot the breasts shape into a 2D space. We show how the breasts subject to a surgery change their representation in this space and provide a cue about the error in this estimation. We believe that the proposed procedure represents a valid solution to evaluate the results of surgeries, since one of the most important goal of the specialists is to symmetrically reconstruct breasts and an objective tool to measure the result is currently missing.

Keywords: 3D scanning, Breast surgery, Histogram of Normals, Principal Component Analysis.

1 Introduction and Motivation

In the last decade 3D scanners have been employed in architecture, engineering, biology, cultural heritage as well as diagnostic medicine and reconstruction surgery [1, 2, 3, 4, 5, 6, 7, 8, 20]. These devices allow doctors to get a detailed virtual model of a human body. The opportunity to acquire body parts shape, including soft tissues like the female human breast, has motivated our conjunct study with the medical specialists in breast reconstruction.

Our main aim is to find a discriminative parametrization of female breast shape i.e., a small set of parameters to objectively describe it. This kind of mathematical representation gives the possibility to easily define accurate metric for breast difference evaluation. This result is very attractive for breast surgeon, since it can be used to develop new tools to assess the symmetry after a breast reconstruction. It could also be an effective strategy to create clear and welldefined breast shape categories.

Currently, the surgeons are routinely used to acquire pictures of the patients, or rather a 2D projection of them. The only way to evaluate the surgery is still based on a photographic comparison using pictures taken before and after the surgery. Nevertheless, 3D scanners capture and store more information, like volume estimation, curvature and so on. The use of these data would enable the specialists to plan and asses the surgery in a more accurate way.

The 3D scanner acquisition of human body parts requires a certain time and skills. Long scanning time, tends to increase the patient stress as well as the amount of noise due to the breath and involuntary micro-movements. Modern hand-held scanners, reduces these problems by allowing low acquisition time. Furthermore it guarantees a sufficiently high quality of the data. Actually, extremely high resolution and accuracy are pointless to capture general shape. Moreover, dense points clouds would affect the processing time. For this reasons we propose to perform dataset acquisition with a fast and low-cost hand-held 3D scanner: Structure Sensor [9]. High portability of hand-held scanners simplifies the operator job, that can easily turn around the patient.

The 3D data have to be processed and simplified to capture just the information that surgeons need for their analysis. In the proposed approach we consider normals orientation to build a compact representation of breast model. To further simplify processed 3D data, Principal Component Analysis (PCA) [10] has been employed. PCA is a popular and valuable approach to reduce the high dimensionality of the datasets and capture just the most significant features. Feature reductions through PCA has already been used in the parametrization process of the human body parts [11, 12]. Concerning the breast shapes, other authors proposed to analyse them either using linear measurements, stationary laser scanner, MRI, X-rays or thermoplastic moulding [13, 14, 15, 16, 17, 18]. Compared to our previous work [20], in this paper we do not employ the planar projections. Our contribution in the field can be summarized in the following points:

- The acquisition of 3D breast models to build a proper dataset and perform significant experiments. At the best of our knowledge there are not available dataset like this.
- The idea to exploit 3D normals to create a compact representation of 3D breast models.
- Time and cost optimization by employing a hand-held 3D scanner.

The remainder of this paper is structured as follows: employed devices and proposed method are described in Section 2. Details on the dataset are provided in subsection 2.1, while the proposed parametrization method is detailed in subsection 2.2. Experimental results are given in Section 3. A final discussion, with some consideration for future works, ends the paper.



Fig. 1. A Structure Sensor clipped onto an iPad. We used the same setting in our acquisitions.

2 Material and methods

The study we conducted is mainly focused on digital shape analysis of breast models to assist breast surgeons for medical and surgical purposes. Our idea is based on three key points: minimally invasive for the patient, use of low cost devices, easy data visualization-&-understanding for people with a medical background.

We employed a 3D scanner with structured infrared light technology that allows us to acquire the information about depth of thousands of points at the same time. The Structure Sensor (Fig. 1) is a hand-held scanner proved to be empirically able to acquire up to 12 meters, although it is recommended a distance in the range 0.4 and 3.5 meters. Its maximum accuracy is 0.5 mm, but worsens when the volume of the area scanned is large. Since the scanner uses infrared rays, it is recommended for indoor usage only. The device is calibrated, that means each 3D model will show its real size. The sensor itself is not able to acquire RGB colour mode information, however it is possible to plug into an iPad and uses the tablet camera to this purpose.

To acquire a breast model, we propose a clinical procedure in which the female patients hold the hands behind and above the head. In this way the operator can move around the breast with the Structure Sensor (which is clipped onto the iPad). Although texture information have been acquired, this has not been used for the present investigation. An example of the model acquired with Structure Sensor is shown in Fig. 2.

Once the model is acquired, it is automatically pre-processed through a 3D processing software (Meshlab [19]), in order to remove noise, isolated vertices and faces. Mesh editing is followed by a manual definition, through cropping, of the Region of Interest (ROI). ROI extraction is a critical part of the proposed procedure. We adopt a simple approach that has been proved to be replicable and reasonable precise. We manually selected the ROI exploiting four anatomical reperces suggested by the breast surgeons (Figs. 2 and 3). In our acquisitions, we scanned both left and right breasts but all of them have been, when needed,



Fig. 2. Example of a textured mesh as it is acquired by the Structure Sensor.



Fig. 3. Definition of ROI through 4 anatomical reperces suggested by the breast surgeons. REMOVE: All right breasts have been mirrored in order to make the dataset right-left side invariant.

vertically mirrored in order to make the dataset right-left side invariant, as shown in Fig. 3.

Each model is saved with the standard OBJ format, which describes the information on vertices, faces and face normals. The average number of vertices is $\sim 1,500$, while the average number of faces is $\sim 4,000$. These models resolution is not extremely high but it is enough to capture information about breast shape, which is the point of this work.

2.1 3D Breast Dataset

After review of the study protocol and formal approval by the internal ethic committee of ASLT (Associazione Santantonese per la Lotta ai Tumori) we gathered a dataset with breasts acquired from different volunteers, aged between 25 and 65, with different shapes and volumes. The breast surgeons put a label on each model, describing size and ptosis of the breast. The severity of ptosis is characterized by evaluating the position of the nipple relative to the infra-mammary fold. Supervised by the doctors, we created a dataset in the following way:

– Main Dataset: is made up of 31 breasts, 17 left and 14 right. To guarantee a proper dataset variability, we have included breasts of different size and ptosis.

Then, in order to test the strenght of the proposed methodology, we selected a patient and acquired her breast several times in pre-operation and post-operation conditions. Hence, two more groups of meshes is distinguishible:

- Group 1: is made by 52 meshes, 26 left and 26 right. Notice that this set of meshes has been acquired by two operators, namely a junior and an expert one, so it can be used to investigate how the proficiency of the operator may change the parameterization.
- Group 2: is made by 16 breasts, 8 left and 8 right.

2.2 Shape Parametrization

In this subsection we present the method employed to process the 3D models in order to parametrize the breast shape. Our idea is to describe each 3D model as histograms of normals. Since normal vectors define the orientation of each model vertex/face, the proposed algorithm starts with a registration step. Actually, although the acquisition device is calibrated, it doesn't have a system to get the correct orientation into the real space (e.g., gravity sensors). Hence, the meshes have initially to be oriented along the same direction and its centroid moved on the origin of a 3D Cartesian coordinate system. As second step, the normal space is clustered and the occurrences for each cluster counted. This descriptor is finally reduced by Principal Component Analysis. The summarized pipeline of proposed method is shown in Fig. 4.

Breast registration As mentioned before, the acquired data have to be rototranslated since the built descriptor depends on normals orientation. This process is automatically performed as described in [20]. First of all the mesh centroid is moved into the origin of a cartesian coordinate system. Subsequently, the average normal is computed to find the rotation matrix, in order to align it along the Z axis. This means, we use the unit vector (0, 0, 1) as reference. Finally, to get the matrix, a closed form named Rodrigues's rotation formula [21] is employed. Specifically, given two vectors u_1 and u_2 , formula computes the rotation to align u_1 to u_2 . In our case $u_1 = averageNormal$ and $u_2 = (0, 0, 1)$.

Bag of Normals After each mesh has been correctly oriented in our coordinate system, we can proceed to obtain a representation of the normals distribution



Fig. 4. Pipeline of the proposed method. Note that PCA is applied on n breast descriptors. Then, the "learnt" transformation matrix is used as model to extract parameters of all the 3D meshes. Additional details are reported in Section 3.

over a suitably quantized grid. Firstly, all the normals are normalized. We divided each normal u for ||u||, in order to get a unit vector. By performing this process, the three components of normal vector (u_x, u_y, u_z) fall in the range [-1, 1]. We linearly quantize the space of each component into 4 levels, in order to obtain $4 \times 4 \times 4 = 64$ different cluster. Finally, each mesh is represented by counting the occurrences in each cluster. This histogram with 64 bins is then in turn normalized to get the final bag of normals descriptor.

Principal Component Analysis (PCA) PCA is a popular statistical method that is commonly used for finding patterns in data of high dimension or reducing such dimensionality. This reduction is more interesting when one wants to extract the main characteristics of complex data. PCA is applied on datasets which are described by several attributes. It is able to find a linear transformation which move the data into another space where the transformed attributes are uncorrelated. The aim is to identify the "Principal Components", or rather a reduced set of attributes which represent the original data [10].

We applied PCA on the 64-d descriptors obtained at the previous step in order to describe each 3D breast with a very small set of parameters, namely 2. This procedure allows us to represent each 3D model as a point in 2D coordinate system where axes are the first two Principal Components. The meaning of these values is discussed in the next section.



Fig. 5. PCA computed on the Main Dataset. (a) Variance Retain of the first 5 principal components. The sum of the first 2 principal components is 77.39%. (b) Plot of the 31 models in the Main Dataset using the first 2 principal components.

3 Results

We computed PCA on the 31 models in the main dataset. Exploiting only the first 2 principal components we obtained a variance retain of 48.04 + 29.35 = 77.39% (Fig. 5(a)) and the models can be represented in a chart, as shown in Fig. 5(b). The breast surgeons confirmed us the evidence of Fig. 5(b): the first 2 principal components seem enough to distinguish characteristic traits of the labeled models, since models are clearly separated in the obtained result.

In order to further assess the soundness of the proposed method we plotted the models of Group 1, exploiting the PCA computed only on the main dataset (Fig. 6(a)). The left breast is clearly distinguishable from the right one, as expected. Once more, using the same principal components, we plotted also the models from Group 2 (Fig. 6(b)). We remark that 3D models in Groups 1 and 2 are all digitization of the breast of the same patient, before and after a surgery, respectively. The mean and standard deviation of models in Groups 1 and 2 have been reported in Table 1. Error ellipses including the 68%, 95% and 99% of the data are contextually shown in Fig. 6(b). The Euclidean distances between centroids of left and right breast clusters for Group 1 and Group 2 are 0.137 and 0.12, respectively. Although the difference between Euclidean distances is tiny, the distance related to the first principal component (the most meaningful, with 48% of variance retain) is way lower: from 0.136 to 0.014. The distance related to the second principal component (29%) of variance retain) is increased from 0.008 to 0.119. So, the results shown in Table 1 and Fig. 6(b) are a confirmation that the right breast and left breast after the surgery (meshes from Group 2) have now a first principal components that has pretty similar mean and variance values, while before the surgery (Group 1) they were different.



Fig. 6. Plots of the models in Group 1 and Group 2 using the first 2 principal components of PCA computed on the Main Dataset. (a) Visual comparison of the principal components of Group 1 between models acquired by the two groups of operators, properly juniors and experts. (b) Comparison of the principal components between Group 1 (pre-surgery) and 2 (post-surgery). Error in the parametrization has been highlighted through error ellipses added on each set of models. Starting from the ellipsis centroid (the mean value of the set), each concentric error ellipsis contains the 68% (σ), the 95% (2 σ) and the 99% (3 σ) of the elements, respectively.

Table 1. Mean and Standard Deviation of models in Group 1 and 2. L stands for Left, R for Right. Each entry is a pair in which the values are related to the first and second principal component, respectively.

	Group 1		Group 2	
	L	R	L	R
Mean	(0.1269, 0.0198)	(-0.0098, 0.0281)	(-0.0124, -0.0352)	(-0.0273, 0.0843)
Stand. Dev.	(0.0127, 0.0262)	(0.0138, 0.0139)	(0.0181, 0.0353)	(0.0258, 0.0129)

The comparative chart with the components of all the digitized breasts is shown in Fig. 7. Some significant cases from Main Dataset are shown in Figs. 8(a) - 8(c), while the patient scanned in Groups 1 and 2 is shown in Figs. 8(d) and 8(e). The breast surgeons confirmed us that the positions of models from these latter sets are coherent with respect to the one of the models from Main Dataset. These results show that the first principal component is strong enough to characterize the shape of a breast, and through the standard deviation computations on Group 1 and 2 we can also give a cue about the error in this estimation.



Fig. 7. Comparison of the first 2 principal components (X and Y axis, respectively) between different datasets. PCA computed on the main dataset, comparison between the main dataset, Group 1 and Group 2.



Fig. 8. Significant acquired models. (a-c) Models from Main Dataset with principal components (-0.17; -0.04), (0; -0.02) and (0.11; -0.01), respectively. They are in the most left, central e right position of the plot of Fig. 5(b). A clear difference about the shape of the breasts can be noticed. (d-e) Patient of Group 1 (pre-surgery) and Group 2 (post-surgery), respectively; note that we considered right breast the one corresponding to the right arm of the patient.

4 Conclusions

In this work we have focused on digital shape analysis of breast models to assist breast specialists for medical and surgical purposes. We fixed three key points for our proposed solution: minimally invasive for the patient approach, use of low cost devices, easy data visualization-&-understanding for people with a medical background. We proposed a clinical procedure in which the female patients hold the hands behind and above the head, while an operator can digitize her breast with a 3D scanner. After a manual ROI definition through cropping, the meshes are automatically processed. The breasts are represented exploiting bag of normals representation, resulting in a 64-d descriptor. A reference dataset has been used to compute PCA on a set of discriminative and different breasts, and the obtained first 2 principal components have been used to plot the breasts into a 2D space. We empirically proved that breasts subjected to a surgery change their representation in this space, and through the variance computations on Group 1 and 2 we also gave a cue about the error in this estimation. We believe that the proposed procedure, assessed by the surgeon, represents a valid solution to evaluate the results of surgeries, since one of the most important goal of the specialists is to symmetrically reconstruct breasts, but an objective tool to measure the result is currently missing. As future works, we planned to augment the ROI extraction phase, which is a critical part of the proposed procedure and requires professionals with a proper know-how of 3D object editing.

Acknowledgment

The authors would like to thank the "Azienda Ospedaliera Cannizzaro", the "Associazione Santantonese per la lotta ai tumori (ASLT)" and the female volunteers for their contribution as models.

References

- D. Huber, B. Akinci, P. Tang, A. Adan, B. Okorn, and X. Xiong. Using laser scanners for modeling and analysis in architecture, engineering, and construction. In *Conference on Information Sciences and Systems (CISS)*, pages 1–6, March 2010.
- [2] Stoll J., P. Novotny, R. Howe, and P. Dupont. Real-time 3d ultrasound-based servoing of a surgical instrument. In *International Conference on Robotics and Automation (ICRA)*, pages 613–618, May 2006.
- [3] A. Bottino, M. De Simone, A. Laurentini, and C. Sforza. A new 3-d tool for planning plastic surgery. *IEEE Transactions on Biomedical Engineering*, 59(12):3439– 3449, 2012.
- [4] P. Treleaven and J. Wells. 3d body scanning and healthcare applications. Computer, 40(7):28–34, July 2007.
- [5] Y. Dai, J. Tian, D. Dong, G. Yan, and H. Zheng. Real-time visualized freehand 3d ultrasound reconstruction based on gpu. *IEEE Transactions on Information Technology in Biomedicine*, 14(6):1338–1345, November 2010.
- [6] F. Stanco, D. Tanasi, D. Allegra, F. L. M. Milotta, G. Lamagna, and G. Monterosso. Virtual anastylosis of greek sculpture as museum policy for public outreach and cognitive accessibility. *Journal of Electronic Imaging*, 26(1), January 2017.
- [7] R. Laing, M. Leon, and J. Isaacs. Monuments visualization: From 3d scanned data to a holistic approach, an application to the city of aberdeen. In *International Conference on Information Visualisation*, pages 512–517, July 2015.

- [8] C. V. Nguyen, J. Fripp, D. R. Lovell, R. Furbank, P. Kuffner, H. Daily, and X. Sirault. 3d scanning system for automatic high-resolution plant phenotyping. In *International Conference on Digital Image Computing: Techniques and Applications (DICTA)*, pages 1–8, Nov 2016.
- [9] Structure Sensor Website http://structure.io/, Last visited April 2017.
- [10] K. Pearson. On lines and planes of closest fit to systems of points in space. *Philosophical Magazine*, 2(6):559–572, 1901.
- [11] B. Allen, B. Curless, and Z. Popovi. The space of human body shapes: reconstruction and parameterization from range scans. In *International Conference on Computer Graphics and Interactive Techniques*, pages 587–594, 2003.
- [12] G. Gallo, G.C. Guarnera, and G. Catanuto. Human breast shape analysis using pca. In Proceedings of the Third International Conference on Bio-inspired Systems and Signal Processing (BIOSIGNALS), 2010.
- [13] D. J. Jr. Smith, W. E. Jr. Palin, V. L. Katch, and J. E. Bennett. Breast volume and anthropomorphic measurements: normal values. *Plastic and reconstructive* surgery, 78(3):331–335, 1986.
- [14] G.M. Farinella, G. Impoco, G. Gallo, S. Spoto, and G. Catanuto. Unambiguous analysis of woman breast breast shape for plastic surgery outcome evaluation. In 4th Conference Eurographics Italian Chapter, 2006.
- [15] G. Catanuto, G. Gallo, G.M. Farinella, G. Impoco, M.B. Nava, A. Pennati, and A. Spano. Breast shape analysis on three-dimensional models. In *Third European Conference on Plastic and Reconstructive Surgery of the Breast*, 2005.
- [16] G. M. Galdino, M. Nahabedian, M. Chiaramonte, J. Z. Geng, S. Klatsky, and P. Manson. Clinical applications of three-dimensional photography in breast surgery. *Plastic and Reconstructive Surgery*, 110(1):58–70, 2002.
- [17] M. Y Nahabedian and G. Galdino. Symmetrical breast reconstruction: is there a role for three-dimensional digital photography? *Plastic and reconstructive surgery*, 112(6):1582–1590, 2003.
- [18] H.Y. Lee, K. Hong, and E.A. Kim. Measurement protocol of womens nude breasts using a 3d scanning technique. *Applied Ergonomics*, 35:353–360, 2004.
- [19] P. Cignoni, M. Callieri, M. Corsini, M. Dellepiane, F. Ganovelli, and G. Ranzuglia. Meshlab: an open-source mesh processing tool. *Eurographics Italian Chapter Conference*, 2008:129–136, 2008.
- [20] G. Gallo, D. Allegra, Y. G. Atani, F. L. M. Milotta, F. Stanco, and G. Catanuto. Breast shape parametrization through planar projections. In J. Blanc-Talon, C. Distante, W. Philips, D. Popescu, and P. Scheunders, editors, *Internation Conference on Advanced Concepts for Intelligent Vision Systems (ACIVS) 2016, Lecce, Italy*, October 2016.
- [21] E. Weisstein. Rodrigues' Rotation Formula: http://mathworld.wolfram.com/rodriguesrotationformula.html, Last visited April 2017.